

Evaluating micellar liquid chromatographic methods on octadecyl particle-based and monolithic columns to predict the skin permeation of drug and cosmetic molecules

Grooten, Yasmine; Marcelis, Quinten; Mangelings, Debby; Vander Heyden, Yvan

Published in:
Journal of Chromatography. A

DOI:
[10.1016/j.chroma.2021.462753](https://doi.org/10.1016/j.chroma.2021.462753)

Publication date:
2022

License:
CC BY-NC-ND

Document Version:
Accepted author manuscript

[Link to publication](#)

Citation for published version (APA):
Grooten, Y., Marcelis, Q., Mangelings, D., & Vander Heyden, Y. (2022). Evaluating micellar liquid chromatographic methods on octadecyl particle-based and monolithic columns to predict the skin permeation of drug and cosmetic molecules. *Journal of Chromatography. A*, 1663, [462753].
<https://doi.org/10.1016/j.chroma.2021.462753>

Copyright

No part of this publication may be reproduced or transmitted in any form, without the prior written permission of the author(s) or other rights holders to whom publication rights have been transferred, unless permitted by a license attached to the publication (a Creative Commons license or other), or unless exceptions to copyright law apply.

Take down policy

If you believe that this document infringes your copyright or other rights, please contact openaccess@vub.be, with details of the nature of the infringement. We will investigate the claim and if justified, we will take the appropriate steps.

1 **Evaluating micellar liquid chromatographic methods on octadecyl particle-based and**
2 **monolithic columns to predict the skin permeation of drug and cosmetic molecules**

3 Yasmine Grooten^a, Quinten Marcelis^b, Debby Mangelings^a, Yvan Vander Heyden^{a*}

4

5 ^a Vrije Universiteit Brussel (VUB), Department of Analytical Chemistry, Applied Chemometrics and Molecular
6 Modelling, Laarbeeklaan 103, B-1090 Brussels, Belgium

7 ^b Vrije Universiteit Brussel (VUB), Department of In Vitro Toxicology and Dermato-Cosmetology, Laarbeeklaan
8 103, B-1090 Brussels, Belgium

9

10 *: Corresponding author

11

12 *E-mail addresses:* yasmine.grooten@vub.be (Y. Grooten), quinten.marcelis@vub.be (Q. Marcelis),
13 debby.mangelings@vub.be (D. Mangelings), yvan.vander.heyden@vub.be (Y. Vander Heyden).

14 **Abstract**

15 A micellar liquid chromatographic method was developed to assist in the modelling of the skin
16 permeability of pharmaceutical and cosmetic compounds. The composition of the mobile phase was
17 determined by means of a two-factor central composite design, after which it was tested on both a
18 particle-based and monolithic column. The latter provided the opportunity to increase the flow rate from
19 1 to 8 mL/min without reaching too high backpressures. The micellar conditions allowed analyzing a
20 large test set of compounds with diverse characteristics with just one mobile-phase composition. The
21 obtained experimental chromatographic descriptors besides two sets of theoretical molecular descriptors
22 were used to model the skin permeability coefficient $\log K_p$, applying multiple linear regression and
23 partial least squares regression approaches. The micellar method on the monolithic column provided
24 useful models with similar or even slightly better performance parameters than the method on the
25 particle-based column. Furthermore, a much faster analysis can be achieved when applying a flow rate
26 of 8 mL/min, making the micellar monolithic method ideal to estimate skin permeability.

27

28 **Keywords**

29 Skin permeability, micellar liquid chromatography, monolithic column, quantitative retention-activity
30 relationship models, quantitative structure-activity relationship models

31 1. Introduction

32 The determination of skin permeability plays an important role in both drug development and risk
33 assessment studies. The diffusion rate of a compound through the skin layers is then determined. The
34 rate of transport is often indicated by the skin permeability coefficient K_p . However, determining this
35 coefficient from *in-vivo* and *in-vitro* experiments often entails certain disadvantages, such as ethical
36 remarks that can be made when using human or animal tests and the time-consuming characteristics of
37 these approaches [1,2]. Moreover, alternative techniques are needed in the context of the replacement,
38 reduction and refinement of animal experiments [2]. Different analytical methods have therefore been
39 applied to predict the skin permeability of compounds, by using a chromatographic descriptor in a
40 quantitative retention-activity relationship (QRAR) model [3–12].

41 Micellar liquid chromatography (MLC) is a type of reversed-phase liquid chromatography
42 (RPLC), in which a surfactant is added to the mobile phase in a concentration exceeding the critical
43 micelle concentration (CMC). In these conditions, micelles are formed in the mobile phase, resulting in
44 a pseudophase which provides an extra dimension of interaction for a compound besides the stationary
45 and mobile phase. Most often sodium dodecyl sulphate (SDS, anionic), cetyltrimethylammonium
46 bromide (CTAB, cationic) or polyoxyethylene-(23)-lauryl ether (Brij-35, non-ionic) are used as
47 surfactant, combined with different stationary phases, such as C18, C8 or cyanopropyl [13,14]. When
48 Brij-35 is combined with a C18 column, this mode is also referred to as biopartitioning micellar
49 chromatography (BMC) [15]. Furthermore, surfactant monomer adsorption to the stationary-phase
50 surface also occurs, causing changes in its polarity (with non-ionic surfactants) or charge (with ionic
51 surfactants), together with a shielding of the residual silanol groups. The addition of organic modifiers,
52 mostly short-chain alcohols or acetonitrile, that form a hybrid micellar mobile phase, may accelerate the
53 elution of compounds and enhance peak shapes. However, their concentration should be limited (often
54 their fraction is in the range 3-15% v/v) given the negative effect on the formation of the micelles [16].
55 This low consumption of organic modifier contributes to the green character of MLC, together with a
56 decrease in solvent costs. Furthermore, the use of a gradient can be avoided because both lipophilic and

57 hydrophilic compounds, covering a broad octanol-water partition coefficient ($\log P$) range, can be
58 determined with the same isocratic run [17].

59 Several studies have already applied a chromatographic descriptor obtained with MLC in QRAR
60 models to predict skin permeability. Waters et al. [18] obtained a good model for the skin permeability
61 based on the micelle-water partition coefficient ($\log P_{mw}$, estimated from experimentally obtained
62 retention factors) and the molecular weight. Their MLC method combined a cyanopropyl column with
63 an SDS-based mobile phase, buffered at pH 5.5. Martínez-Pla et al. [19] applied a similar BMC approach
64 and used the retention factor and melting point to model the skin permeability. Furthermore, this
65 research group successfully predicted the pH effect on the skin permeability of compounds from BMC
66 results [20]. A BMC system containing some acetonitrile in the mobile phase was used by Dobričić et
67 al. [21] to predict the skin and corneal permeabilities of 17β -carboxamide steroids, using the obtained
68 retention factors in artificial neural network (ANN), multiple linear regression (MLR) and partial least
69 squares (PLS) quantitative structure-retention relationship (QSRR) models. After comparison, the PLS-
70 QSRR model showed the best predictive properties.

71 Monolithic columns are composed of a single piece of porous material, characterized by a
72 bimodal structure of macropores and mesopores [22,23]. Because of the highly porous characteristics
73 of these columns, lower backpressures are acquired, which allows working at higher flow rates and
74 achieving faster analyses (five to ten times faster than with particle-based columns) [24]. Detroyer et al.
75 [25] compared the use of a monolithic and particle-based column, both with and without a micellar
76 mobile phase based on SDS as surfactant, to predict $\log P$ (an indicator for membrane permeability).
77 With this 'fast' micellar monolithic liquid chromatographic method the flow could be increased to
78 9 mL/min, maintaining a good correlation with membrane permeability. Furthermore, Lu et al. [26] have
79 applied BMC successfully on a monolithic column to model the blood-brain barrier penetration,
80 showing its potential as a fast and high-throughput method.

81 In previous research, the chromatographic retention on a C18 column showed little added value
82 to skin permeability models relative to models with only theoretical descriptors [10]. Therefore, the aim
83 of this study was to develop a micellar liquid chromatographic method on the same column type, and

84 additionally on a monolithic column, to improve the skin permeability prediction of pharmaceutical and
85 cosmetic compounds. With MLC, a diverse set of compounds may be analyzed with one mobile-phase
86 composition, due to the modification of the stationary phase by the surfactant monomers. Consequently,
87 there is no need for extrapolation to a theoretical retention factor without organic modifier ($\log k_w$) as is
88 often the case in RPLC. From a two-factor central composite design approach, the best fraction of
89 organic modifier (1-propanol) and concentration of surfactant (SDS) in the mobile phase were
90 determined. The selected mobile phase was then used to screen a test set of 58 pharmaceutical and
91 cosmetic compounds on both column types. The monolithic column was applied to obtain a fast and
92 high-throughput MLC method. This approach has already been suitable to estimate intestinal absorption
93 [25] and blood-brain barrier penetration [26], and will in this study be used for the prediction of skin
94 permeability. Afterwards, the chromatographic data will be combined with molecular descriptors to
95 model the skin permeability coefficient, applying MLR and PLS modelling approaches.

96 **2. Materials and methods**

97 *2.1. Reagents*

98 Methanol (MeOH, VWR Chemicals, Leuven, Belgium) and 1-propanol (Fisher Scientific,
99 Loughborough, UK) were both HPLC grade. Sodium dodecyl sulfate (SDS), the anionic surfactant in
100 the mobile phase, was purchased from Sigma Aldrich (Steinheim, Germany). Sodium acetate (Sigma
101 Aldrich) was used to prepare a 0.05 M acetate buffer pH 5.5, adjusting the pH with 1 M hydrochloric
102 acid (Fisher Scientific). The test set consisted of the following 58 compounds: 17 α -
103 hydroxyprogesterone, 2,4,6-trichlorophenol, 2,4-dichlorophenol, 2-amino-4-nitrophenol, 2-nitro-p-
104 phenylenediamine, 4-amino-2-nitrophenol, acetylsalicylic acid, aminopyrine, atropine, benzyl alcohol,
105 chloroxylenol, chlorpheniramine maleate, cortexolone, cortexone, corticosterone, cortisolone, diclofenac,
106 ephedrine.HCl, ethyl nicotinate, flurbiprofen, ibuprofen, indomethacin, ketoprofen, lidocaine, m-cresol,
107 methyl nicotinate, m-nitrophenol, naproxen, o-chlorophenol, o-cresol, paracetamol, p-cresol, piroxicam,
108 p-nitrophenol, p-phenylenediamine, prednisolone, progesterone, salicylic acid, testosterone, thymol,
109 triamcinolone, triamcinolone acetonide (all Sigma Aldrich), amylobarbitol and barbitol (Bios Coutelier,
110 Brussels, Belgium), benzoic acid, phenol, resorcinol, thiourea, β -naphthol (Merck, Darmstadt,

111 Germany), caffeine, methyl-4-hydroxybenzoate (Fluka, Neu-Ulm, Switzerland), hydrocortisone (Certa,
112 Braine-l'Alleud, Belgium), estrone (Diosynth, Oss, The Netherlands), antipyrine, estriol, haloperidol,
113 phenobarbitone and β -estradiol (gifts from unknown origin). The minimum purity of these compounds
114 was 95%. Ultrapure water was provided by an Arium Pro UV system (Sartorius Stedim Biotech,
115 Göttingen, Germany).

116 2.2. *Chromatographic conditions*

117 The HPLC system consisted of an L-7200 autosampler with a 100 μ L loop, L-7100 pump, D-7000
118 interface and L-7400 UV detector from Merck-Hitachi (Tokyo, Japan). An external Igloo-Cil column
119 oven (Amchro, Hattersheim, Germany) was used to keep the column temperature at 25°C. All
120 compounds were analyzed at a wavelength of 220 nm. D-7000 HPLC System Manager software
121 (Merck-Hitachi, 1994–2001, version 4.1) was used to process the obtained chromatographic data. The
122 first disturbance of the baseline signal was used as the dead time. Buffers were vacuum-filtered through
123 0.20 μ m membranes (Sartorius Stedim Biotech) and all mobile phases were degassed in an ultrasonic
124 bath before use.

125 2.3. *Two-factor central composite design to optimize the mobile phase*

126 Mobile phases consisting of SDS in 0.05 M acetate buffer pH 5.5 (mimicking the pH of the skin) and 1-
127 propanol were studied. A flow rate of 1.0 mL/min and an injection volume of 20 μ L were applied. A
128 smaller test set of 15 compounds, covering the log P range of the complete test set (-1.13 to 4.45), was
129 selected: antipyrine, caffeine, cortexone, cortisone, diclofenac, ibuprofen, ketoprofen, lidocaine, methyl-
130 4-hydroxybenzoate, paracetamol, prednisolone, progesterone, testosterone, thymol and triamcinolone.
131 A two-factor central composite design requiring nine experiments was applied to optimize the
132 concentration of the surfactant SDS (x_1) and the fraction of organic modifier 1-propanol (x_2) in the
133 mobile phase. The range of the SDS concentration (0.01 - 0.15 M) was determined based on other
134 research [27–29], keeping in mind the CMC of SDS. The experimental domain for 1-propanol was
135 limited by the maximal amount that preserves the formation of the micelles (15% v/v 1-propanol) [30].
136 The two factors were explored on five levels ($-\alpha$, -1, 0, +1, $+\alpha$), of which the corresponding values can

137 be found in **Table 1**. For every mobile phase, the retention factor k of the 15 compounds was determined.
138 For each compound second-order models were built to model the retention factor k as a function of the
139 factors, according to the following equation:

$$140 \quad k = \beta_0 + \beta_1 x_1 + \beta_2 x_2 + \beta_{12} x_1 x_2 + \beta_{11} x_1^2 + \beta_{22} x_2^2 \quad (\text{Eq. 1})$$

141 in which x_1 represents the concentration of SDS (in M), x_2 the percentage of 1-propanol and β_i the
142 coefficients of the model. With this equation, the retention factors could be predicted for the entire
143 experimental domain.

144 *2.4. Particle-column experiments*

145 An Xterra RP18 column (150 mm x 4.6 mm i.d., 5 μm) from Waters (Milford, MA, USA) was used for
146 the particle-column experiments. A stock solution of 1.0 mg/mL of the standards was prepared in
147 MeOH. The stock solutions were diluted 10 times with a 0.05 M SDS in 0.05 M acetate buffer pH 5.5
148 to obtain a final concentration of 0.1 mg/mL. The stock and working solutions were kept in the fridge
149 until analysis (maximum duration of 2 months). A flow rate of 1 mL/min was applied and 10 μL of the
150 standards was injected.

151 *2.5. Monolithic-column experiments*

152 A Chromolith Performance RP-18e column (100 mm x 4.6 mm i.d.) from Merck was used for the
153 monolithic-column experiments. The flow was increased from 1 to 8 mL/min with steps of 1 mL/min
154 (taking into account the maximal pressure of the column). An injection volume of 10 μL was applied.
155 Standards of 1 mg/mL were prepared in MeOH, after which a dilution to 0.1 mg/mL was made in 0.08 M
156 SDS in 0.05 M acetate buffer pH 5.5. Standard solutions were kept in the fridge until analysis.

157 *2.6. Analysis of the entire test set*

158 The test set of 58 compounds was analyzed with the mobile phase, consisting of SDS in 0.05 M acetate
159 buffer pH 5.5 and 1-propanol, as organic modifier, in the quantities determined from the central
160 composite design results. To assess the repeatability of injection, three compounds, caffeine (fast

161 eluting), m-nitrophenol (intermediate retention) and 2,4,6-trichlorophenol (slow eluting), were injected
162 six times.

163 2.7. Data sources, software and data processing

164 Retention factors k were calculated as $(t_r - t_0)/t_0$, in which t_r stands for the retention time and t_0 for the
165 dead time. The calculations and plots for the optimization of the mobile phase were made with m-files
166 in MATLAB® 2014a (The Mathworks, Natick, MA, USA). The scatter plots were created with
167 GraphPad Prism (GraphPad Software, San Diego, CA, USA, version 8.4.3).

168 The skin permeability coefficients, $\log K_p$, were obtained from validated *in-vitro* tests reported in
169 the literature [31–35]. Although it is not ideal to combine K_p values from different sources, it is difficult
170 to avoid because of the lack of extended skin permeability data sets. A number of physicochemical,
171 geometrical and topological descriptors, e.g. virtual $\log P$, molecular weight and number of atoms, were
172 calculated with Vega ZZ version 3.1.2.29 [36]. The melting point was derived from PubChem [37]. An
173 additional set of molecular descriptors (a total of 1666 descriptors) was obtained from the E-Dragon
174 software. These descriptors belong to different descriptor classes, such as constitutional indices,
175 functional group counts, molecular properties, topological indices and atom-centred fragments [38,39].
176 (Nearly) constant variables and descriptor pairs with a high correlation ($r > 0.95$) were removed, keeping
177 the variable which showed the highest correlation to the $\log K_p$ values.

178 The Vega ZZ software was used to build the MLR models applying the ‘automatic linear regression’
179 module. When a descriptor showed an r^2 below 0.10 with the skin permeability coefficient, it was not
180 included in the model. Furthermore, highly correlated descriptors (variance inflation factor $VIF > 5$,
181 with $VIF = 1/(1-r^2)$) were not considered together in the MLR models. Models were built including one
182 to seven descriptors. The software provided a ranking of the best models, from which the best model
183 including the chromatographic descriptor was selected. An overview of these models is provided in the
184 Supplementary material.

185 MATLAB® was used to compose stepwise MLR and PLS models. For the first modelling approach,
186 forward selections are followed by backwards deletions of descriptors until a partial F-test determines

187 that the model is no longer improved by the addition or deletion of descriptors. For the best PLS model,
188 the number of PLS factors is determined from the lowest root mean squared error of (leave-one-out)
189 cross validation (RMSECV) value. For all models, the RMSECV and the root mean squared error of
190 calibration (RMSEC) are calculated and used to validate the models, because lower values correspond
191 to better models. The relative percentages of these parameters were calculated using the average $\log K_p$
192 values. The determination coefficient r^2 (between the $\log K_p(\text{experimental})$ and $\log K_p(\text{predicted})$) was
193 also used to assess the models.

194 **3. Results and discussion**

195 *3.1. Selection of the mobile-phase composition*

196 A small test set of 15 compounds was analyzed on the particle-based column according to the two-factor
197 central composite design with nine different mobile-phase compositions, varying in concentration of
198 SDS (surfactant) and percentage of 1-propanol (organic modifier) (see **Fig. 1**). The measured retention
199 factors for each mobile phase can be found in **Table 2**. All compounds could be analyzed with every
200 mobile-phase composition, even though the range of $\log P$ values was quite wide. It can be noticed that
201 both an increase in SDS concentration as in fraction of 1-propanol led to an overall decrease in retention
202 of the compounds. However, only MP 3 (0.03 M SDS + 12.8% v/v 1-propanol) and MP 6 (0.08 M SDS
203 + 15% v/v 1-propanol) showed the same elution sequence, indicating that small partition changes can
204 occur when changing the mobile-phase composition.

205 Building the quadratic polynomial models of Eq. 1 allowed predicting the response, i.e. the retention
206 factors, for the entire experimental domain. **Fig. 2** shows an overlay plot of the predicted retention
207 factors for caffeine (one of the earliest eluting compounds) and thymol (the last eluting compound). It
208 is difficult to find an optimal mobile-phase composition, and we look for a compromise between the
209 different responses. It is more important to indicate an area in the experimental domain in which the
210 retention factor of caffeine is above 1 (to avoid co-elution with the injection peak) and the k value for
211 thymol is reasonably low (to keep the analysis time within an acceptable time frame). Within this
212 restricted area, the preference was given to a tested mobile phase, instead of interpolating in the domain.
213 This resulted in three remaining mobile-phase compositions: MP 4 (0.08 M SDS without 1-propanol),

214 MP 5 (0.08 M SDS + 7.5% v/v 1-propanol) and MP 7 (0.13 M SDS + 2.2% v/v 1-propanol). Because
215 the log k values of these three mobile phases are highly correlated (r between 0.988 – 0.998), they seem
216 to contain similar information. Therefore, the mobile phase in the center of the domain (MP 5),
217 consisting of 0.08 M SDS in 0.05 M acetate buffer pH 5.5 with 7.5% v/v 1-propanol, was chosen, since
218 the surroundings of this point were explored in the design, in contrast to the mobile phases at the borders
219 of the experimental domain.

220 3.2. Analysis of the entire test set on the particle-based column

221 After selection of the mobile-phase composition, the test set of 58 compounds was analyzed at the
222 chosen conditions. The resulting retention factors ($k_{particle}$) can be found in **Table 3**, together with the
223 skin permeability coefficients ($\log K_p$), octanol-water partition coefficients ($\log P$) and molecular
224 weights (MW) of all compounds. The retention factors ranged between 0.45 and 140. However, the last
225 eluting compound (haloperidol) showed an excessively high retention compared to the other analytes.
226 Since haloperidol is completely positively ionized at pH 5.5, it is likely to interact extensively with the
227 negatively charged SDS monomers adsorbed to the stationary phase. This compound was considered as
228 an outlier for the modelling, leading to a new retention factor range of 0.45 – 38.9. The repeatability of
229 injection was confirmed with a standard deviation below 0.1%.

230 When evaluating the relationship between the skin permeability coefficients, $\log K_p$, and the
231 retention factors, $k_{particle}$, a better correlation was obtained with the $k_{particle}$ values ($r = 0.475$) than with
232 the $\log k_{particle}$ values ($r = 0.357$). However, in both cases the retention factors on their own were
233 insufficient to model the skin permeability. Therefore, two sets of molecular descriptors were considered
234 to further improve the models, i.e. descriptors calculated with the Vega ZZ and E-Dragon software.
235 First, MLR models were built with the molecular descriptors from the Vega ZZ software (see **Tables**
236 **S1** and **S2** in the Supplementary material for an overview of the models containing $k_{particle}$ and $\log k_{particle}$,
237 respectively). When increasing the number of descriptors in these models, an improvement in the fit
238 (lower RMSEC value) is noticed, which is also expected. Initially, the same trend is seen for the
239 predictive capacities (RMSECV) of these models. However, after including a certain number of
240 descriptors, the model becomes susceptible to overfitting, leading to an increase in the RMSECV values.

241 The best MLR model is therefore a compromise between fit and prediction, which in this case led to an
242 optimal model with four descriptors, including the $\log k_{particle}$, number of atoms, virtual $\log P$ and
243 melting point (see Eq. 2 in **Table 4**). It should be noted that the best MLR model including $k_{particle}$
244 provided similar results.

245 When resorting to stepwise MLR modelling with E-Dragon descriptors, Eq. 3 (**Table 4**) was
246 obtained with nine descriptors and the $\log k_{particle}$.

$$\begin{aligned} \log K_p = & -2.19(\pm 0.44) - 0.36(\pm 0.03) RDF020e + 0.51(\pm 0.07) C-025 + 0.66(\pm 0.12) \log k_{particle} + \\ & 1.88(\pm 0.31) Lop + 0.25(\pm 0.05) nCconj - 1.45(\pm 0.30) GATS2p + 0.78(\pm 0.20) Mor11m - \\ & 6.68(\pm 2.24) RBF - 1.01(\pm 0.30) GIp - 7.68(\pm 3.36) JGI5 \quad (\text{Eq. 3}) \end{aligned}$$

$$250 \quad RMSEC = 0.329 \text{ (12.4\%)}, RMSECV = 0.399 \text{ (15.0\%)}, r^2 = 0.93, n = 57$$

251 This model showed a clear improvement compared to the MLR model with the Vega ZZ descriptors,
252 both in terms of fit (r^2 and RMSEC) and predictive capabilities (RMSECV). The predicted $\log K_p$ values
253 versus the experimental are plotted in **Fig. 3**, in which slightly more deviation is noticed for the lower
254 $\log K_p$ values. The definition of the selected E-Dragon descriptors can be consulted in **Table S3** of the
255 Supplementary material. The $k_{particle}$ values were not selected for the stepwise MLR model including the
256 E-Dragon descriptors.

257 Furthermore, PLS models were constructed with both the $\log k_{particle}$ and the Vega ZZ or E-Dragon
258 descriptors. The best PLS models included the number of PLS factors resulting in the lowest RMSECV
259 value. The Vega ZZ descriptor set led to a model with six PLS factors and somewhat similar
260 performance parameters to the MLR model built with the same descriptor set (RMSEC = 0.694 or
261 26.1%, RMSECV = 0.813 or 30.5% and $r^2 = 0.69$). With the E-Dragon descriptor set, nine PLS factors
262 led to the best model (RMSEC = 0.421 or 15.8%, RMSECV = 0.730 or 27.4% and $r^2 = 0.89$). Although
263 the RMSEC value for this model was better, the predictive properties (RMSECV) showed little
264 improvement compared to the other PLS model. Furthermore, it is noticed that the influence of the
265 chromatographic descriptor on the PLS models is rather low. Overall, the best model, which includes

266 the chromatographic descriptor from the particle-based column, was obtained applying stepwise MLR
267 modelling on the E-Dragon descriptor set.

268 3.3. Analysis of the entire test set on the monolithic column

269 The mobile phase composition determined in 3.1. was also applied to analyze the test set on a monolithic
270 column. The flow rate was increased from 1 to 8 mL/min with steps of 1 mL/min. With this flow rate
271 increase, the pressure rises with about 22 bar per added mL/min. Therefore, the highest flow rate that
272 could be applied, keeping in mind the maximal pressure of the column (200 bar), was reached at
273 8 mL/min. An overview of the individual retention factors at each flow rate can be consulted in **Table**
274 **S4** of the Supplementary material. The average retention factors (k_m) at the different flow rates can be
275 consulted in **Table 3**, together with their standard deviation. The average k_m values ranged between 0.02
276 and 43.58, with again haloperidol showing the highest value. This compound was again regarded as an
277 outlier for the modelling, with the subsequent highest retention factor being 9.90 (chlorpheniramine
278 maleate). Furthermore, acetylsalicylic acid and salicylic acid often showed little to no retention ($k <$
279 0.05), leading to their elimination from the modelling when using the $\log k$ values. The repeatability of
280 injection was below 1.5%. The average relative standard deviation over the different flow rates was
281 8.70%. However, the correlation between the retention factors at 1 and 8 mL/min was 0.9998, indicating
282 that there was no loss of information when increasing the flow rate. Therefore, the retention factors of
283 the lowest and highest flow rates were used to model the skin permeability. In this way, it could be
284 assessed whether similar models are obtained when increasing the flow rate.

285 When taking a look at the correlation between the retention factors obtained on the monolithic
286 column and the skin permeability coefficients, it can be noticed that the retention factors at 1 mL/min,
287 k_{m1} , and 8 mL/min, k_{m8} , show similar r values with the $\log K_p$ values ($r = 0.458$ and 0.447 , respectively).
288 Further, although the correlation between $\log K_p$ and $\log k_{m1}$ was less good ($r = 0.380$), a better
289 correlation was seen with $\log k_{m8}$ ($r = 0.470$). Once more, these retention parameters without the use of
290 theoretical descriptors were insufficient to model the skin permeability.

291 Theoretical descriptors were added besides the chromatographic to improve the models. An
292 overview of the MLR models, including the retention factors from the lowest and highest flow rates (1
293 and 8 mL/min, respectively) and the Vega ZZ descriptors, ranging from one to seven descriptors, can
294 be found in **Tables S5-S8** in the Supplementary material. When comparing these models, the best
295 RMSECV is in both cases obtained by combining the $\log k_m$ with three Vega ZZ descriptors (Eqs. 4 and
296 5 in **Table 5**). For both models the number of atoms (*Atoms*), virtual $\log P$ and number of hydrogen
297 bond donors (*HbDon*) were selected besides the chromatographic descriptor. The model including
298 $\log k_{m8}$ (Eq. 5) was slightly better, but it should be noticed that only 55 compounds can be used, since
299 salicylic acid and acetylsalicylic acid showed no retention ($k < 0.05$, of which no meaningful logarithmic
300 value is obtained).

301 For the stepwise MLR models built with the E-Dragon descriptors, slightly better models were
302 obtained when using the $\log k$ values instead of the k values (Eqs. 6-9 in **Table 5**). A number of common
303 descriptors is found in these four models, i.e. *RDF020e*, *C-025* and *Glu*. The best model was again
304 acquired using $\log k_{m8}$ (Eq. 9), showing very good results for the RMSEC, RMSECV and r^2 (see **Fig. 4**).

$$\begin{aligned} \log K_p = & -3.33(\pm 0.38) - 0.35(\pm 0.03) \text{RDF020e} + 0.39(\pm 0.07) \text{C-025} + 0.80(\pm 0.17) \log k_{m8} - \\ & 0.86(\pm 0.30) \text{Glu} + 2.21(\pm 0.35) \text{Lop} + 0.21(\pm 0.07) \text{EEig11d} - 0.14(\pm 0.06) \text{ALOGPS_logS} + \\ & 0.56(\pm 0.21) \text{Mor11m} - 13.25(\pm 2.83) \text{RBF} + 1.67(\pm 0.58) \text{MATS2e} - 0.61(\pm 0.29) \text{Mor18m} \end{aligned}$$

(Eq. 9)

$$\text{RMSEC} = 0.337 \text{ (12.6\%)}, \text{RMSECV} = 0.412 \text{ (15.4\%)}, r^2 = 0.93, n = 55$$

310 However, with 11 descriptors in total, this model was also the most complex. A description of the
311 selected E-Dragon descriptors can be found in **Table S3** of the Supplementary material.

312 For the PLS modelling with the Vega ZZ descriptors, the retention factors k_m for a flow rate of
313 1 mL/min (RMSEC = 0.683 or 25.6%, RMSECV = 0.797 or 29.9% and $r^2 = 0.70$) and 8 mL/min
314 (RMSEC = 0.683 or 25.6%, RMSECV = 0.807 or 30.3% and $r^2 = 0.70$) in both cases provided the best
315 models with seven PLS factors. Thus, similar results were obtained at both flow rates. Using the E-
316 Dragon descriptors, nine PLS factors were selected, leading to an improved model with $\log k_{m1}$ (RMSEC

317 = 0.421 or 15.8%, RMSECV = 0.730 or 27.4% and $r^2 = 0.89$), while at a flow of 8 mL/min k_{m8} (RMSEC
318 = 0.421 or 15.8%, RMSECV = 0.736 or 27.6% and $r^2 = 0.89$) gives the best PLS model. Although the
319 fit of these models clearly showed an improvement relative to the PLS model with the Vega ZZ
320 descriptors, the predictive capacities were similar as well as to the MLR models built with the Vega ZZ
321 descriptors. Again, it should be mentioned that the influence of the chromatographic descriptor is rather
322 low for these PLS models.

323 In conclusion, the models with the chromatographic descriptors from 1 and 8 mL/min showed
324 similar performance parameters, indicating that the same model quality can be obtained at increased
325 flow rate. Thus, a faster method can be used without a loss of information. The best model with a
326 chromatographic descriptor from the monolithic column was from the stepwise MLR approach and
327 includes $\log k_{m8}$ and E-Dragon descriptors.

328 3.4. Comparison of the column types

329 A test set of 58 compounds was analyzed on both a particle and a monolithic column, using the same
330 micellar mobile phase. On the particle column a flow rate of 1 mL/min was applied, while the monolithic
331 column allowed an increase of the flow from 1 to 8 mL/min (steps of 1 mL/min). When comparing the
332 retention factors on both columns (see **Fig. 5**), it can be noticed that the values on the particle column
333 were overall much higher than on the monolithic column. However, the correlation between these two
334 columns was lower than expected, i.e. $r = 0.789$ (without haloperidol), meaning that for some
335 compounds different elution mechanisms were at work.

336 In terms of analysis time, the elution of the most retained compound (haloperidol) on the monolithic
337 column ($t_r = 56$ min) only took about half the time of the analysis on the particle column ($t_r = 126$ min)
338 at the same flow rate (1 mL/min). It should be noted that shorter analysis times on the monolithic column
339 are already expected because of its shorter column length. When increasing the flow rate on the
340 monolithic column, the retention time of haloperidol further decreased to 7.75 min at a flow rate of
341 8 mL/min, which was almost seven times faster than the result at 1 mL/min on this column type. The
342 skin permeability models including the chromatographic descriptor from both column types are

343 compared. In addition, to explore the added value of these chromatographic descriptors, the obtained
344 models were compared to models built with only theoretical descriptors in a previous study [10].

345 When comparing the models set up with the different retention descriptors, it can be noticed that the
346 MLR models applying Vega ZZ descriptors showed similar parameters (Eqs. 2, 4 and 5). In all three
347 cases, three molecular descriptors (besides $\log k$) were selected for the best model, with the number of
348 atoms and virtual $\log P$ as common descriptors. Using the particle-column retention in the model, the
349 melting point was selected as fourth descriptor, while the number of hydrogen bond donors was selected
350 for the monolithic column. When comparing these models to the best MLR models containing only
351 Vega ZZ descriptors (four descriptors, RMSEC = 0.690 or 25.7%, RMSECV = 0.752 or 28.0% and r^2
352 = 0.69) [10], minimal improvement is noticed with the current models containing the retention
353 information.

354 Further, the stepwise MLR models containing E-Dragon descriptors, besides $\log k_{particle}$ (Eq. 3) or
355 for the monolithic column either k_m or $\log k_m$ (Eqs. 6-9), were compared. A total of ten descriptors was
356 used for the models including the results from the particle or the monolithic column at a flow of
357 1 mL/min, while at 8 mL/min on the monolithic column nine descriptors were selected when using k_{m8}
358 and eleven with $\log k_{m8}$. These stepwise MLR models showed very good values for RMSEC, RMSECV
359 and r^2 , with the best result coming from the analyses on the particle column. Furthermore, an
360 improvement in the performance parameters is noticed in comparison to the best stepwise MLR model
361 with only theoretical descriptors from an earlier study (stepwise MLR model with ten E-Dragon
362 descriptors led to RMSEC = 0.378 or 14.1%, RMSECV = 0.452 or 16.8% and $r^2 = 0.91$) [10].

363 Finally, when considering the PLS models, those built with the Vega ZZ descriptors show similar
364 performance parameters as the MLR models using the same descriptor set and this for both column
365 types. An improvement in the RMSEC values was seen for the PLS models composed with the E-Dragon
366 descriptors, for which the models from the particle-based and monolithic column (both at 1 and
367 8 mL/min) showed great similarities. This could be mainly attributed to the theoretical descriptors,
368 because the influence of the chromatographic descriptor was rather low. In comparison to the PLS
369 models built with only theoretical descriptors, more PLS factors were each time selected when the

370 retention descriptors from this study were added. The inclusion of the MLC retention results led to an
371 improved fit compared to the PLS model based on only Vega ZZ descriptors, although no improvement
372 in the predictive capabilities was observed (five PLS factors resulting in RMSEC = 0.757 or 28.2%,
373 RMSECV = 0.807 or 30.0% and $r^2 = 0.63$). On the other hand, the PLS models based on E-Dragon
374 descriptors showed a clear improvement when adding the chromatographic descriptors from MLC (six
375 PLS factors, RMSEC = 0.674 or 25.1%, RMSECV = 0.860 or 32.0% and $r^2 = 0.72$) [10].

376 The overall best models were thus obtained with the stepwise MLR approach, applying E-Dragon
377 descriptors. The models including $\log k_{particle}$ (Eq. 3) or $\log k_{m8}$ (Eq. 9) show comparable results. Both
378 models presented an added value of the chromatographic descriptor in comparison to the corresponding
379 pure *in-silico* models, and are thus most suitable to apply in future skin permeability applications.

380 4. Conclusions

381 In this study, the retention obtained with micellar liquid chromatographic methods was used to model
382 the skin permeability of pharmaceutical and cosmetic compounds. A limited test set was used to
383 determine the optimal concentration of SDS and the percentage of 1-propanol in the mobile phase, using
384 an experimental design approach. A mobile phase consisting of 0.08 M SDS in 0.05 M acetate buffer
385 with 7.5% v/v 1-propanol was selected. These conditions were then applied to analyze a larger test set
386 on two column types: a particle-based and a monolithic, the latter having the advantage of allowing an
387 increase in flow rate to 8 mL/min without generating too high backpressures. Although there were some
388 dissimilarities in retention between these two columns, the use of the retention factors ($\log k$) provided
389 similar models for the skin permeability. The addition of Vega ZZ descriptors provided the best MLR
390 models with $\log P$, number of atoms and melting point or number of hydrogen bond donors, i.e.
391 descriptors that easily can be related to skin permeability processes. The stepwise MLR models
392 containing E-Dragon descriptors were in this regard more abstract to interpret, but provided the best
393 models. The PLS models built with E-Dragon descriptors also provided a good fit, but showed less good
394 predictive abilities. Furthermore, these PLS models should be nuanced by the rather small importance
395 of the chromatographic descriptor. Because both columns provided models with often similar quality,
396 the monolithic column is preferred because of its faster operating conditions. Additionally, all models

397 were compared with skin permeability models containing only theoretical descriptors from a previous
398 study, in which the same modelling approaches were applied. It was observed that the addition of the
399 retention descriptor from the MLC methods provided improved models. In conclusion, the micellar
400 method on the monolithic column offers a fast approach to effectively estimate the skin permeability of
401 pharmaceutical and cosmetic compounds.

402

403 **Acknowledgments**

404 Y.G. is funded by a Ph.D. fellowship of the Research Foundation Flanders (FWO) [grant 11D3518N].

405

406 **Conflict of Interest**

407 The authors declare that they have no conflict of interest.

409 **Table 1.** The levels and factors varied in the two-factor central composite design.

Level	Factor	
	$x_1 = \text{concentration SDS}$ (M)	$x_2 = \text{fraction 1-propanol}$ (%)
$-\alpha$	0.01	0
-1	0.03	2.2
0	0.08	7.5
+1	0.13	12.8
$+\alpha$	0.15	15.0

410

411 **Table 2.** The measured retention factors k with the nine mobile-phase (MP) compositions of the
 412 experimental design. The SDS concentration (M) and fraction of 1-propanol (%) were specified for each
 413 mobile phase.

Compound	MP 1	MP 2	MP 3	MP 4	MP 5	MP 6	MP 7	MP 8	MP 9
	0.01 M 7.5%	0.03 M 2.2%	0.03 M 12.8%	0.08 M 0%	0.08 M 7.5%	0.08 M 15.0%	0.13 M 2.2%	0.13 M 12.8%	0.15 M 7.5%
Antipyrine	1.81	2.91	0.87	2.89	1.43	1.15	1.72	0.68	1.23
Caffeine	1.16	1.69	0.59	2.00	1.09	0.90	1.32	0.50	1.03
Cortexone	66.2	26.6	15.4	11.9	10.5	8.14	6.80	4.57	6.08
Cortisone	15.7	12.5	4.58	6.30	4.93	3.35	3.58	2.09	3.11
Diclofenac	85.4	75.7	27.2	37.9	27.1	13.1	22.3	8.69	16.1
Ibuprofen	76.8	64.2	26.1	35.8	22.0	12.9	19.6	7.83	13.2
Ketoprofen	9.23	13.6	4.20	10.8	5.85	3.11	6.09	2.32	4.51
Lidocaine	134	57.8	28.7	25.1	18.1	13.4	13.3	6.92	9.74
Methyl-4- hydroxybenzoate	19.4	19.0	8.98	12.3	10.1	7.33	8.08	4.86	6.97
Paracetamol	1.19	1.31	0.70	1.44	1.08	1.05	1.13	0.59	1.02
Prednisolone	19.9	15.0	5.44	7.81	5.39	3.73	4.16	2.24	3.32
Progesterone	136	41.1	33.3	15.7	19.2	16.5	10.2	9.02	9.78
Testosterone	72.7	26.1	19.2	10.6	12.1	10.4	6.69	5.78	7.03
Thymol	196	105	57.8	47.9	39.7	30.1	28.8	16.5	22.7
Triamcinolone	8.10	7.54	2.84	3.83	3.53	2.42	2.47	1.52	2.41

414 **Table 3.** The octanol-water partition coefficients ($\log P$), skin permeability coefficients ($\log K_p$),
 415 molecular weights (MW) and the retention factors on both the particle-based ($k_{particle}$) and monolithic
 416 column (\bar{k}_m , average for the different flow rates, along with the standard deviation s).

Compound	$\log P^a$	MW^a	$\log K_p^b$	$k_{particle}$	$\bar{k}_m (s)$
17 α -Hydroxyprogesterone	1.84	330.46	-3.22	13.35	2.72 (0.09)
2,4,6-Trichlorophenol	3.94	197.45	-1.23	38.65	7.15 (0.21)
2,4-Dichlorophenol	3.18	163.00	-1.22	28.11	5.51 (0.15)
2-Amino-4-nitrophenol	1.39	154.12	-3.18	6.00	0.80 (0.04)
2-Nitro-p-phenylenediamine	0.78	153.14	-3.30	4.43	1.05 (0.04)
4-Amino-2-nitrophenol	1.22	154.12	-2.55	5.53	1.32 (0.05)
Acetylsalicylic acid	1.10	180.16	-2.14 [33]	0.46	0.02 (0.04)
Aminopyrine	1.57	231.29	-2.99	3.63	1.55 (0.06)
Amylobarbitol	1.97	226.27	-2.64	11.51	3.42 (0.10)
Antipyrine	1.26	188.23	-4.18	1.46	0.66 (0.03)
Atropine	2.14	289.37	-5.07	11.47	4.29 (0.13)
Barbital	0.95	184.19	-3.96	2.24	0.55 (0.03)
Benzoic acid	1.24	122.12	-1.52	1.07	0.19 (0.03)
Benzyl alcohol	1.34	108.14	-2.22	3.71	1.11 (0.05)
Caffeine	-0.25	194.19	-2.80	1.08	0.48 (0.03)
Chloroxylenol	3.06	156.61	-1.23	28.81	6.11 (0.18)
Chlorpheniramine (maleate)	3.86	274.79	-2.66	23.33	9.90 (0.29)
Cortexolone	0.97	346.46	-4.12	8.39	1.81 (0.06)
Cortexone	1.92	330.46	-3.35	10.55	2.80 (0.10)
Corticosterone	0.82	346.46	-3.19	6.81	1.80 (0.07)
Cortisone	-0.12	360.44	-5.00	4.97	1.11 (0.04)
Diclofenac	4.45	296.15	-1.74	26.87	5.67 (0.22)
Ephedrine.HCl	1.73	165.23	-2.22	17.57	8.12 (0.21)
Estriol	2.30	288.38	-4.40	16.87	0.56 (0.04)
Estrone	3.18	270.37	-2.44	27.10	3.20 (0.11)
Ethyl nicotinate	1.35	151.16	-2.20	4.99	3.52 (0.09)
Flurbiprofen	3.88	244.26	-0.34	19.96	5.04 (0.19)
Haloperidol	3.75	375.86	-4.04 [34]	140.43	43.58 (1.23)
Hydrocortisone	0.01	362.46	-5.52	5.19	1.17 (0.04)
Ibuprofen	3.20	206.28	-0.24	22.08	7.28 (0.27)

Indomethacin	4.04	357.79	-1.30	16.61	3.57 (0.16)
Ketoprofen	2.23	254.28	-1.23	6.39	1.28 (0.07)
Lidocaine	3.01	234.34	-1.70 [35]	18.21	7.30 (0.21)
m-Cresol	2.09	108.14	-1.82	11.26	2.39 (0.07)
Methyl nicotinate	0.93	137.14	-2.49	2.75	2.08 (0.08)
Methyl-4-hydroxybenzoate	1.36	152.15	-2.04	10.10	1.50 (0.05)
m-Nitrophenol	2.21	139.11	-2.25	15.51	2.07 (0.06)
Naproxen	3.23	230.26	-1.42	10.61	2.29 (0.09)
o-Chlorophenol	2.40	128.56	-1.48	14.84	2.86 (0.08)
o-Cresol	2.07	108.14	-1.80	12.63	2.48 (0.08)
Paracetamol	1.07	151.16	-3.35	1.08	0.16 (0.03)
p-Cresol	2.16	108.14	-0.92	11.09	2.44 (0.08)
Phenobarbitone	1.49	232.24	-3.35	6.40	1.67 (0.05)
Phenol	1.59	94.11	-1.71	6.70	1.35 (0.04)
Piroxicam	1.59	331.35	-2.47	4.64	1.14 (0.06)
p-Nitrophenol	2.17	139.11	-2.25	13.34	1.84 (0.06)
p-Phenylenediamine	0.23	108.14	-3.62	4.57	1.44 (0.06)
Prednisolone	-0.45	360.44	-4.35	5.44	1.33 (0.11)
Progesterone	2.85	314.46	-2.82	19.12	6.55 (0.19)
Resorcinol	1.18	110.11	-3.62	1.97	0.34 (0.03)
Salicylic acid	0.96	138.12	-2.20	0.45	0.05 (0.03)
Testosterone	2.48	288.42	-3.40	12.06	2.58 (0.09)
Thiourea	-0.65	76.12	-4.02 [32]	0.69	0.12 (0.03)
Thymol	3.23	150.22	-1.28	38.94	7.34 (0.20)
Triamcinolone	-1.13	394.43	-5.40	3.53	0.58 (0.03)
Triamcinolone acetonide	1.40	434.50	-4.69	11.44	2.11 (0.07)
β -estradiol	3.37	272.38	-2.37	29.57	1.65 (0.07)
β -naphthol	2.61	144.17	-1.55	23.12	4.43 (0.13)

417 ^a (Virtual) $\log P$ and MW [$\text{g}\cdot\text{mol}^{-1}$] were calculated with Vega ZZ software.

418 ^b The $\log K_p$ values [$\text{cm}\cdot\text{h}^{-1}$] were mostly obtained from a validated database [31]. Other sources are
419 indicated.

420 **Table 4.** The best MLR models containing the (logarithm of the) retention factors obtained on the particle-based column ($k_{particle}$), along with the standard error
 421 on the coefficients, together with their root mean squared error of calibration (RMSEC), root mean squared error of cross validation (RMSECV), both with their
 422 relative values (calculated using the average $\log K_p$ value), and the determination coefficient (r^2) values.

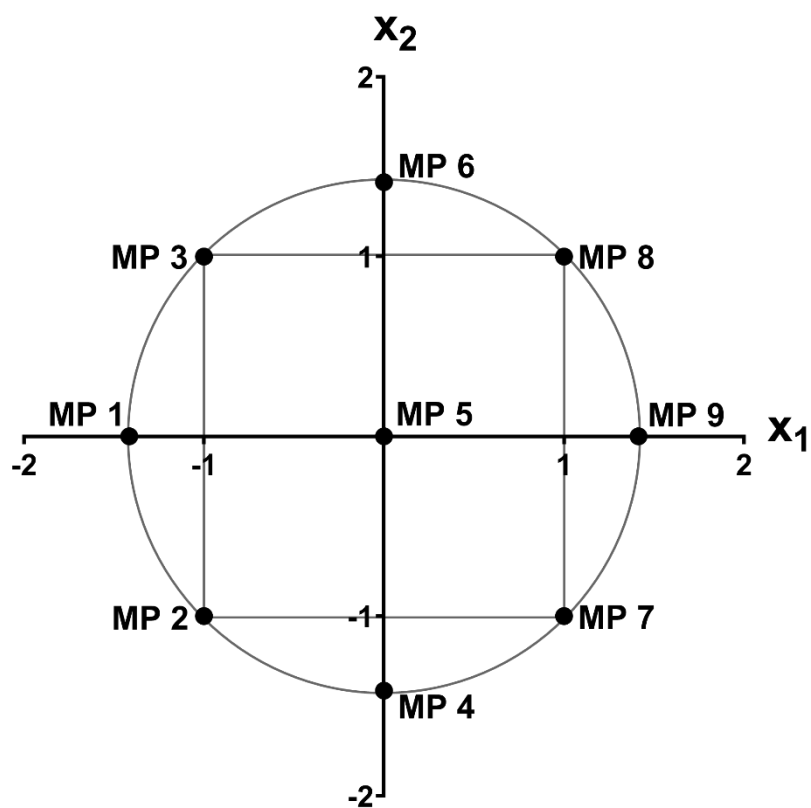
RMSEC	RMSECV	r^2	n	Equation
0.675 (25.3%)	0.733 (27.5%)	0.71	57	$\log K_p = -2.36(\pm 0.29) - 0.20(\pm 0.33) \log k_{particle} - 0.026(\pm 0.009) Atoms + 0.64(\pm 0.12) Virtual \log P - 0.0040(\pm 0.0019) Melting \ point$ (Eq. 2)
0.329 (12.4%)	0.399 (15.0%)	0.93	57	$\log K_p = -2.19(\pm 0.44) - 0.36(\pm 0.03) RDF020e + 0.51(\pm 0.07) C-025 + 0.66(\pm 0.12) \log k_{particle} + 1.88(\pm 0.31) Lop + 0.25(\pm 0.05) nCconj - 1.45(\pm 0.30) GATS2p + 0.78(\pm 0.20) Mor11m - 6.68(\pm 2.24) RBF - 1.01(\pm 0.30) G1p - 7.68(\pm 3.36) JGI5$ (Eq. 3)

423 Description of the selected E-Dragon descriptors: see **Table S3**.

424 **Table 5.** The best MLR models containing the (logarithm of) retention factor obtained on the monolithic column at flow rates of 1 mL/min (k_{m1}) and 8 mL/min
 425 (k_{m8}), along with the standard error on the coefficients, together with their performance parameters.

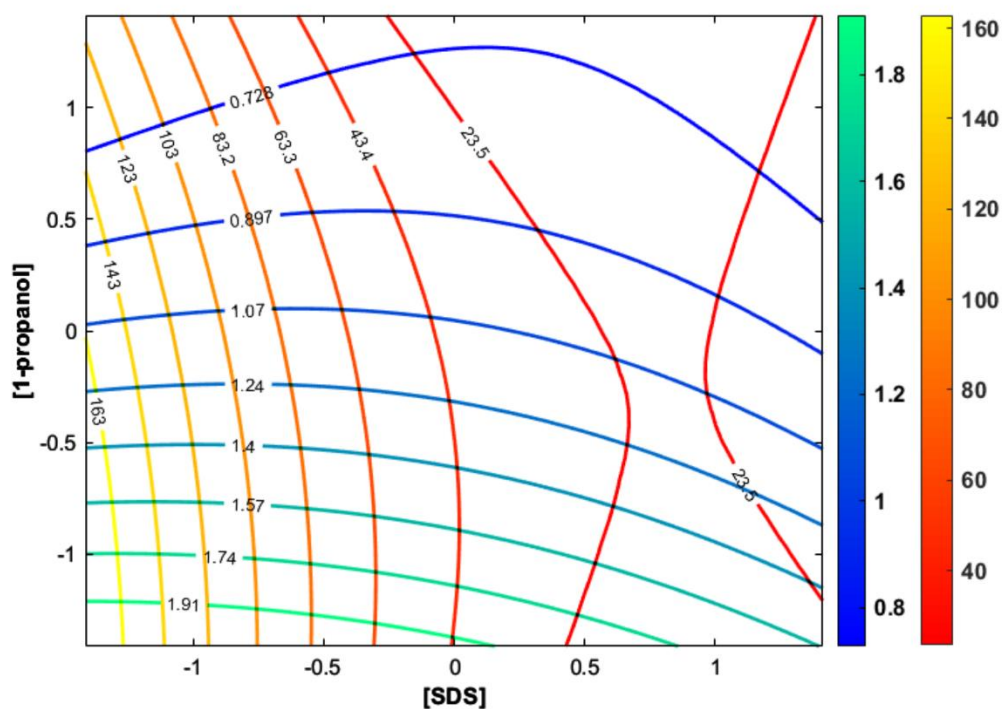
RMSEC	RMSECV	r^2	n	Equation
0.676 (25.4%)	0.735 (27.6%)	0.70	57	$\log K_p = -2.15(\pm 0.35) + 0.17(\pm 0.28) \log k_{m1} - 0.040(\pm 0.007) Atoms + 0.52(\pm 0.11) Virtual \log P - 0.20(\pm 0.10) HbDon$ (Eq. 4)
0.670 (25.0%)	0.734 (27.4%)	0.72	55	$\log K_p = -2.18(\pm 0.36) + 0.46(\pm 0.33) \log k_{m8} - 0.041(\pm 0.007) Atoms + 0.47(\pm 0.12) Virtual \log P - 0.18(\pm 0.11) HbDon$ (Eq. 5)
0.345 (13.0%)	0.425 (16.0%)	0.92	57	$\log K_p = -8.26(\pm 1.96) - 0.40(\pm 0.03) RDF020e + 0.43(\pm 0.07) C-025 + 0.13(\pm 0.03) k_{m1} - 0.98(\pm 0.27) Glu + 11.37(\pm 2.46) JGI4 - 1.65(\pm 0.42) GATS2e + 1.20(\pm 0.23) Lop + 1.69(\pm 0.49) BEHm1 + 0.88(\pm 0.37) MATS3m + 0.17(\pm 0.07) EEig11d$ (Eq. 6)
0.342 (12.8%)	0.408 (15.3%)	0.92	57	$\log K_p = -1.83(\pm 0.41) - 0.42(\pm 0.03) RDF020e + 0.36(\pm 0.08) C-025 + 0.85(\pm 0.13) \log k_{m1} - 0.96(\pm 0.28) Glu + 2.22(\pm 0.35) Lop + 0.20(\pm 0.07) EEig11d - 9.75(\pm 2.30) RBF - 1.81(\pm 0.48) GATS2e - 1.28(\pm 0.31) Mor18m + 23.03(\pm 11.16) JGI8$ (Eq. 7)
0.377 (14.2%)	0.459 (17.2%)	0.91	57	$\log K_p = -0.86(\pm 0.38) - 0.23(\pm 0.03) RDF020e + 0.40(\pm 0.07) C-025 + 0.12(\pm 0.03) k_{m8} - 1.20(\pm 0.31) Glu - 2.17(\pm 0.55) GATS2p - 1.89(\pm 0.46) E2s - 0.20(\pm 0.05) nCs + 0.054(\pm 0.017) H-046 + 1.59(\pm 0.59) GATS2m$ (Eq. 8)
0.337 (12.6%)	0.412 (15.4%)	0.93	55	$\log K_p = -3.33(\pm 0.38) - 0.35(\pm 0.03) RDF020e + 0.39(\pm 0.07) C-025 + 0.80(\pm 0.17) \log k_{m8} - 0.86(\pm 0.30) Glu + 2.21(\pm 0.35) Lop + 0.21(\pm 0.07) EEig11d - 0.14(\pm 0.06) ALOGPS_{logS} + 0.56(\pm 0.21) Mor11m - 13.25(\pm 2.83) RBF + 1.67(\pm 0.58) MATS2e - 0.61(\pm 0.29) Mor18m$ (Eq. 9)

426 Description of the selected E-Dragon descriptors: see **Table S3**.



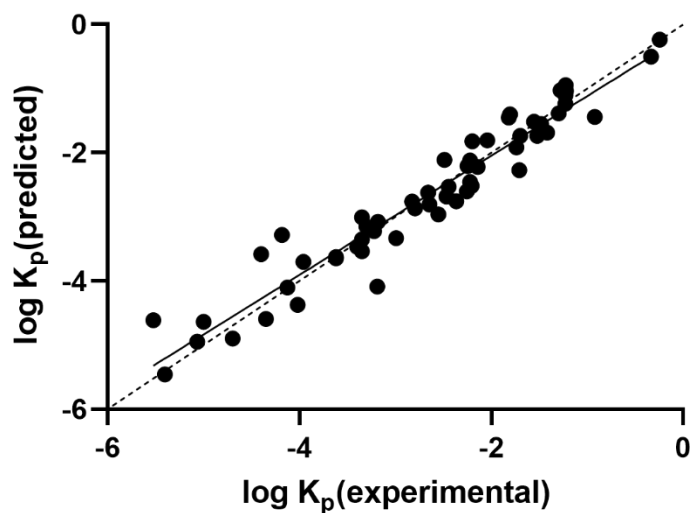
428

429 **Fig. 1.** Visual representation of the two-factor central composite design to optimize the concentration of
430 SDS (x_1) and the fraction of 1-propanol (x_2) in the mobile phase. The labelled dots indicate the nine
431 tested mobile-phase (MP) compositions. The levels are defined in **Table 1**.



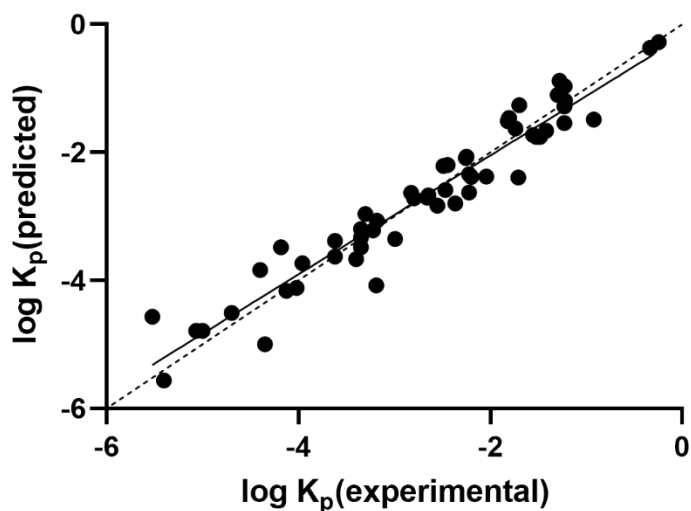
432

433 **Fig. 2.** Overlay of the contour plots for the predicted retention factors of caffeine (horizontal lines in
 434 blue/green) and thymol (vertical lines in red/yellow).



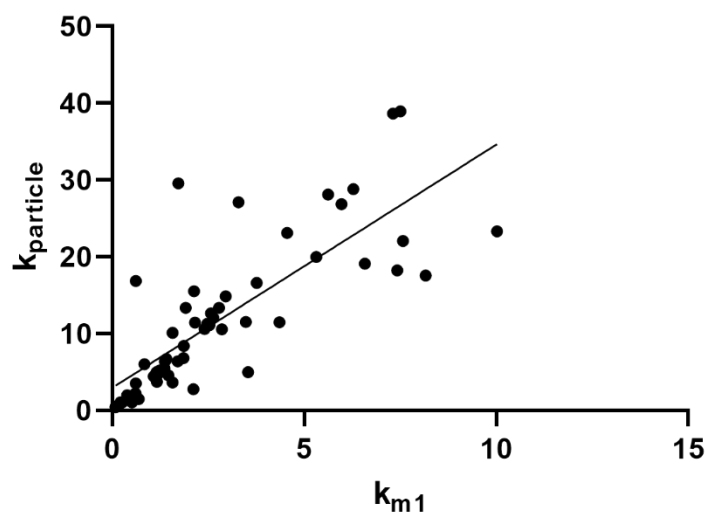
435

436 **Fig. 3.** The predicted skin permeability coefficients $\log K_p$, based on the results from the stepwise MLR
 437 model, including the $\log k_{particle}$ and E-Dragon descriptors (Eq. 3), versus the experimental values,
 438 together with the regression line (solid line) and the bisector ($y = x$, dashed line).



439

440 **Fig. 4.** The predicted $\log K_p$ values from the stepwise MLR model containing the $\log k_{m8}$ on the
 441 monolithic column and E-Dragon descriptors (Eq. 9), versus the experimental. The regression line (solid
 442 line) and bisector (dashed line) are also shown.



443

444 **Fig. 5.** The retention factors (without haloperidol) obtained on the particle column ($k_{particle}$) versus the
 445 retention factors on the monolithic column (k_{m1}), together with the regression line.

446 **References**

- 447 [1] J. Kielhorn, S. Melching-Kollmuß, I. Mangelsdorf, *Environmental Health Criteria 235: Dermal*
448 *Absorption*, World Health Organization Press, Geneva, 2006.
- 449 [2] R. Neupane, S.H.S. Boddu, J. Renukuntla, R.J. Babu, A.K. Tiwari, *Alternatives to biological*
450 *skin in permeation studies: current trends and possibilities*, *Pharmaceutics*. 12 (2020) 152.
451 <https://doi.org/10.3390/PHARMACEUTICS12020152>.
- 452 [3] F. Barbato, B. Cappello, A. Miro, M.I. La Rotonda, F. Quaglia, *Chromatographic indexes on*
453 *immobilized artificial membranes for the prediction of transdermal transport of drugs*, *II*
454 *Farmaco*. 53 (1998) 655–661. [https://doi.org/10.1016/S0014-827X\(98\)00082-2](https://doi.org/10.1016/S0014-827X(98)00082-2).
- 455 [4] A. Nasal, M. Sznitowska, A. Buciński, R. Kaliszan, *Hydrophobicity parameter from high-*
456 *performance liquid chromatography on an immobilized artificial membrane column and its*
457 *relationship to bioactivity*, *J. Chromatogr. A*. 692 (1995) 83–89. [https://doi.org/10.1016/0021-](https://doi.org/10.1016/0021-9673(94)00689-7)
458 [9673\(94\)00689-7](https://doi.org/10.1016/0021-9673(94)00689-7).
- 459 [5] M. Turowski, R. Kaliszan, *Keratin immobilized on silica as a new stationary phase for*
460 *chromatographic modelling of skin permeation*, *J. Pharm. Biomed. Anal.* 15 (1997) 1325–1333.
461 [https://doi.org/10.1016/S0731-7085\(96\)02009-2](https://doi.org/10.1016/S0731-7085(96)02009-2).
- 462 [6] Y. Wang, J. Sun, H. Liu, J. Liu, L. Zhang, K. Liu, Z. He, *Predicting skin permeability using*
463 *liposome electrokinetic chromatography*, *Analyst*. 134 (2009) 267–272.
464 <https://doi.org/10.1039/b807497f>.
- 465 [7] M. Turowski, R. Kaliszan, *Collagen immobilised on silica derivatives as a new stationary phase*
466 *for HPLC*, *Biomed. Chromatogr.* 12 (1998) 187–192. [https://doi.org/10.1002/\(SICI\)1099-](https://doi.org/10.1002/(SICI)1099-0801(199807/08)12:4<187::AID-BMC727>3.0.CO;2-2)
467 [0801\(199807/08\)12:4<187::AID-BMC727>3.0.CO;2-2](https://doi.org/10.1002/(SICI)1099-0801(199807/08)12:4<187::AID-BMC727>3.0.CO;2-2).
- 468 [8] E. Lázaro, C. Ràfols, M.H. Abraham, M. Rosés, *Chromatographic estimation of drug disposition*
469 *properties by means of immobilized artificial membranes (IAM) and C18 columns*, *J. Med.*
470 *Chem.* 49 (2006) 4861–4870. <https://doi.org/10.1021/jm0602108>.

- 471 [9] M. Hidalgo-Rodríguez, S. Soriano-Meseguer, E. Fuguet, C. Ràfols, M. Rosés, Evaluation of the
472 suitability of chromatographic systems to predict human skin permeation of neutral compounds,
473 *Eur. J. Pharm. Sci.* 50 (2013) 557–568. <https://doi.org/10.1016/j.ejps.2013.04.005>.
- 474 [10] Y. Grooten, A. Sych, D. Mangelings, Y. Vander Heyden, Comparison of in-silico modelling and
475 reversed-phase liquid chromatographic retention on an octadecyl silica column to predict skin
476 permeability of pharmaceutical and cosmetic compounds, *J. Pharm. Biomed. Anal.* 201 (2021)
477 114095. <https://doi.org/10.1016/j.jpba.2021.114095>.
- 478 [11] S. Soriano-Meseguer, E. Fuguet, A. Port, M. Rosés, Estimation of skin permeation by liquid
479 chromatography, *ADMET DMPK.* 6 (2018) 140–152. <https://doi.org/10.5599/admet.512>.
- 480 [12] A.W. Sobańska, J. Robertson, E. Brzezińska, Application of RP-18 TLC retention data to the
481 prediction of the transdermal absorption of drugs, *Pharmaceuticals.* 14 (2021) 147.
482 <https://doi.org/10.3390/PH14020147>.
- 483 [13] M.J. Ruiz-Ángel, S. Carda-Broch, J.R. Torres-Lapasió, M.C. García-Álvarez-Coque, Retention
484 mechanisms in micellar liquid chromatography, *J. Chromatogr. A.* 1216 (2009) 1798–1814.
485 <https://doi.org/10.1016/j.chroma.2008.09.053>.
- 486 [14] M.C. García-Alvarez-Coque, M.J. Ruiz-Angel, E. Peris-García, Liquid Chromatography |
487 Micellar Liquid Chromatography, in: P. Worsfold, A. Townshend, C. Poole, M. Miró (Eds.),
488 *Encyclopedia of Analytical Science*, third ed., Elsevier, Amsterdam, The Netherlands, 2019, pp.
489 133–142.
- 490 [15] L. Escuder-Gilabert, J.J. Martínez-Pla, S. Sagrado, R.M. Villanueva-Camañas, M.J. Medina-
491 Hernández, Biopartitioning micellar separation methods: modelling drug absorption, *J.*
492 *Chromatogr. B.* 797 (2003) 21–35. [https://doi.org/10.1016/S1570-0232\(03\)00606-8](https://doi.org/10.1016/S1570-0232(03)00606-8).
- 493 [16] C.F. Poole, The Column in Liquid Chromatography, in: *The Essence of Chromatography*,
494 Elsevier Science, Amsterdam, The Netherlands, 2003, pp. 267–429.

- 495 [17] R.N. El-Shaheny, M.H. El-Maghrabey, F.F. Belal, Micellar liquid chromatography from green
496 analysis perspective, *Open Chem.* 13 (2015) 877–892. <https://doi.org/10.1515/chem-2015-0101>.
- 497 [18] L.J. Waters, Y. Shahzad, J. Stephenson, Modelling skin permeability with micellar liquid
498 chromatography, *Eur. J. Pharm. Sci.* 50 (2013) 335–340.
499 <https://doi.org/10.1016/j.ejps.2013.08.002>.
- 500 [19] J.J. Martínez-Pla, Y. Martín-Biosca, S. Sagrado, R.M. Villanueva-Camañas, M.J. Medina-
501 Hernández, Biopartitioning micellar chromatography to predict skin permeability, *Biomed.*
502 *Chromatogr.* 17 (2003) 530–537. <https://doi.org/10.1002/bmc.281>.
- 503 [20] J.J. Martínez-Pla, Y. Martín-Biosca, S. Sagrado, R.M. Villanueva-Camañas, M.J. Medina-
504 Hernández, Evaluation of the pH effect of formulations on the skin permeability of drugs by
505 biopartitioning micellar chromatography, *J. Chromatogr. A.* 1047 (2004) 255–262.
506 <https://doi.org/10.1016/j.chroma.2004.07.011>.
- 507 [21] V. Dobričić, K. Nikolic, S. Vladimirov, O. Čudina, Biopartitioning micellar chromatography as
508 a predictive tool for skin and corneal permeability of newly synthesized 17 β -carboxamide
509 steroids, *Eur. J. Pharm. Sci.* 56 (2014) 105–112. <https://doi.org/10.1016/j.ejps.2014.02.007>.
- 510 [22] G. Guiochon, Monolithic columns in high-performance liquid chromatography, *J. Chromatogr.*
511 *A.* 1168 (2007) 101–168. <https://doi.org/10.1016/j.chroma.2007.05.090>.
- 512 [23] P.G. Wang, *Monolithic Chromatography and its Modern Applications*, first ed., ILM
513 Publications, St Albans, UK, 2010.
- 514 [24] K. Cabrera, Applications of silica-based monolithic HPLC columns, *J. Sep. Sci.* 27 (2004) 843–
515 852. <https://doi.org/10.1002/jssc.200401827>.
- 516 [25] A. Detroyer, Y. Vander Heyden, K. Reynaert, D.L. Massart, Evaluating “fast” micellar
517 monolithic liquid chromatography for high-throughput quantitative structure-retention
518 relationship screening, *Anal. Chem.* 76 (2004) 1903–1908. <https://doi.org/10.1021/ac030339e>.

- 519 [26] R. Lu, J. Sun, Y. Wang, H. Li, J. Liu, L. Fang, Z. He, Characterization of biopartitioning micellar
520 chromatography system using monolithic column by linear solvation energy relationship and
521 application to predict blood-brain barrier penetration, *J. Chromatogr. A.* 1216 (2009) 5190–5198.
522 <https://doi.org/10.1016/j.chroma.2009.05.007>.
- 523 [27] I. Rapado-Martínez, M.C. García-Alvarez-Coque, R.M. Villanueva-Camañas, Liquid
524 chromatographic procedure for the evaluation of β -blockers in pharmaceuticals using hybrid
525 micellar mobile phases, *J. Chromatogr. A.* 765 (1997) 221–231. [https://doi.org/10.1016/S0021-9673\(96\)00919-3](https://doi.org/10.1016/S0021-9673(96)00919-3).
- 527 [28] L.J. Waters, Y. Shahzad, J.C. Mitchell, pH effects in micellar liquid chromatographic analysis
528 for determining partition coefficients for a series of pharmaceutically related compounds, *Curr.*
529 *Pharm. Anal.* 8 (2012) 272–277. <https://doi.org/10.2174/157341212801619379>.
- 530 [29] A. Detroyer, Y. Vander Heyden, S. Carda-Broch, M.C. García-Alvarez-Coque, D.L. Massart,
531 Quantitative structure-retention and retention-activity relationships of β -blocking agents by
532 micellar liquid chromatography, *J. Chromatogr. A.* 912 (2001) 211–221.
533 [https://doi.org/10.1016/s0021-9673\(01\)00577-5](https://doi.org/10.1016/s0021-9673(01)00577-5).
- 534 [30] M.J. Ruiz-Angel, R.D. Caballero, E.F. Simó-Alfonso, M.C. García-Alvarez-Coque, Micellar
535 liquid chromatography: suitable technique for screening analysis, *J. Chromatogr. A.* 947 (2002)
536 31–45. [https://doi.org/10.1016/S0021-9673\(01\)01595-3](https://doi.org/10.1016/S0021-9673(01)01595-3).
- 537 [31] B.E. Vecchia, A.L. Bunge, Skin Absorption Databases and Predictive Equations, in: R.H. Guy,
538 J. Hadgraft (Eds.), *Transdermal Drug Delivery*, Marcel Dekker, New York, 2003, pp. 57–141.
- 539 [32] K.T. Hoang, *Dermal Exposure Assessment: Principles and Applications*, Environmental
540 Protection Agency, Office of Health and Environmental Assessment, EPA/600/8–91/011B,
541 Washington DC, USA, 1992.
- 542 [33] I.T. Degim, W.J. Pugh, J. Hadgraft, Skin permeability data: anomalous results, *Int. J. Pharm.* 170
543 (1998) 129–133. [https://doi.org/10.1016/S0378-5173\(98\)00113-6](https://doi.org/10.1016/S0378-5173(98)00113-6).

- 544 [34] A.F. Azarbayjani, H. Lin, C.W. Yap, Y.W. Chan, S.Y. Chan, Surface tension and wettability in
545 transdermal delivery: a study on the in-vitro permeation of haloperidol with cyclodextrin across
546 human epidermis, *J. Pharm. Pharmacol.* 62 (2010) 770–778.
547 <https://doi.org/10.1211/jpp.62.06.0014>.
- 548 [35] J. Thomas, S. Majumdar, S. Wasdo, A. Majumdar, K.B. Sloan, The effect of water solubility of
549 solutes on their flux through human skin in vitro: an extended Flynn database fitted to the
550 Roberts-Sloan equation, *Int. J. Pharm.* 339 (2007) 157–167.
551 <https://doi.org/10.1016/j.ijpharm.2007.02.031>.
- 552 [36] A. Pedretti, L. Villa, G. Vistoli, VEGA - an open platform to develop chemo-bio-informatics
553 applications, using plug-in architecture and script programming, *J. Comput. Aided. Mol. Des.* 18
554 (2004) 167–173. <https://doi.org/10.1023/b:jcam.0000035186.90683.f2>.
- 555 [37] S. Kim, J. Chen, T. Cheng, A. Gindulyte, J. He, S. He, Q. Li, B.A. Shoemaker, P.A. Thiessen,
556 B. Yu, L. Zaslavsky, J. Zhang, E.E. Bolton, PubChem 2019 update: improved access to chemical
557 data, *Nucleic Acids Res.* 47 (2019) D1102–D1109. <https://doi.org/10.1093/nar/gky1033>.
- 558 [38] I.V. Tetko, J. Gasteiger, R. Todeschini, A. Mauri, D. Livingstone, P. Ertl, V.A. Palyulin, E.V.
559 Radchenko, N.S. Zefirov, A.S. Makarenko, V.Y. Tanchuk, V.V. Prokopenko, Virtual
560 computational chemistry laboratory – design and description, *J. Comput. Aided. Mol. Des.* 19
561 (2005) 453–463. <https://doi.org/10.1007/s10822-005-8694-y>.
- 562 [39] I.V. Tetko, Computing chemistry on the web, *Drug Discov. Today.* 10 (2005) 1497–1500.
563 [https://doi.org/10.1016/S1359-6446\(05\)03584-1](https://doi.org/10.1016/S1359-6446(05)03584-1).